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1 **Effect of low-intensity pulsed ultrasound after intraoral vertical ramus osteotomy**

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1 **Abstract**

2 **Objective.** The present study investigated the effect of Low-Intensity Pulsed Ultrasound (LIPUS) on long-
3 term osseous healing of the cleavage space between bone fragments after intraoral vertical ramus osteotomy
4 (IVRO).

5 **Study Design.** Patients undergoing IVRO were randomly selected to be in the LIPUS group (n=12) or
6 control group (n=9) after surgery. LIPUS treatments were applied daily to the cleavage space between bone
7 fragments for 3 weeks. We observed three-dimensional quantitative color mapping of the whole mandible
8 created by computed tomography (CT) data at one month, six months, and one year postoperatively. Based
9 on CT values, the color grades were classified as D1 to D5 using Misch criteria. We then calculated mean
10 CT values and rated each color grade in different selection ranges.

11 **Results.** The mean CT values of the LIPUS group were significantly higher than that of the control group
12 at one month, six months and one year postoperatively ($p<0.01$). The color grades of the cleavage between
13 bone fragments increased from D5 to D1 over time.

14 **Conclusion.** Our results indicated that LIPUS promoted osseous healing after IVRO, improving bone
15 density and offering clinical benefits.

16

1 **Introduction**

2 Many surgical techniques are performed for the treatment of mandibular prognathism. Sagittal
3 split ramus osteotomy (SSRO) and intraoral vertical ramus osteotomy (IVRO) are the most frequently used
4 methods of mandibular ramus osteotomy. Both surgical techniques have risks and benefits. The advantage
5 of IVRO over SSRO is technical simplicity; there is a lower incidence of injury or damage to the inferior
6 alveolar nerve, shorter operation time, and the ability to reposition the condyle.¹ However, IVRO has a
7 prolonged duration of postoperative intermaxillary fixation (IMF) required due to the absence of rigid bone
8 fixation, causing a relatively long time between the operation and osseous healing. IMF prevents an early
9 return to usual dietary life, causes a prolonged functional impairment to patients and most severely, can
10 compromise the airway when vomiting. Several reports showed mandibular prognathism by IVRO can be
11 with supported by intraoral fixation with a plate or screw instead of IMF.² However, it is important to
12 promote osseous healing regardless of the use of IMF.

13 Low-Intensity Pulsed Ultrasound (LIPUS) is known to promote bone healing. In orthopedic
14 surgery, it is a clinically established treatment method used to accelerate long bone fracture healing and is
15 a medical service covered by health insurance in Japan. There has been great interest due to its portability,
16 ease of handling, and noninvasive nature.³ On the other hand, Schandelmaier S et al.⁴ demonstrated that
17 LIPUS does not improve outcomes important to patients and probably has no effect on radiographic bone
18 healing in patients with fresh fractures. However, they described that the applicability to other types of
19 fracture or osteotomy is open to debate. We previously demonstrated that cells within mandibular fracture

1 haematomas contribute to mandibular fracture healing and that the osteogenic activity of human mandibular
2 fracture haematoma-derived cells (MHCs) is enhanced by LIPUS stimulation.^{5,6} We provided significant
3 evidence for the potential utility of the clinical application of LIPUS to accelerate mandibular fracture
4 healing. Some recent studies have shown significant effect of LIPUS on mandibular defects and fractures.⁷⁻
5 ⁹ However, the therapeutic effect of LIPUS on the healing process after IVRO still remains unclear.

6 Recently, we demonstrated osseous healing in the cleavage between bone fragments after IVRO
7 using Computed Tomography (CT) values in the axial CT images.¹⁰ The CT values between bone fragments
8 significantly increased at one month, six months, one year and two years after surgery. However,
9 radiographic assessment is limited by 2D interpretations of a 3D structure, and no report so far has
10 investigated detailed osseous healing of the whole mandible in three dimensions. The purpose of this study
11 was to determine the effect of LIPUS on the healing of osteotomy sites after IVRO and observe the long-
12 term osseous healing of the cleavage space between bone fragments after IVRO surgery using quantitative
13 3D analyses of clinical CT data. We hypothesized that LIPUS can accelerate mandibular osseous healing
14 similar to HMCs studied previously.

15

16 **Materials and Methods**

17 *Ethics*

18 The present study was a prospective cohort study. This study has been conducted in full accordance
19 with the World Medical Association Declaration of Helsinki. All procedures used in this research were

1 approved by the Ethical Committee of Kobe University Hospital (approval number: No.789) and informed
2 consent was obtained from each patient.

3 *Participants*

4 The inclusion criteria were (i) patients who had mandibular prognathism and received mandibular
5 set-back surgery with bilateral IVRO, (ii) no previous orthognathic surgery and no maxillary surgery, (iii)
6 no history of facial fracture or jaw trauma, and (iv) patients available for all evaluation time points. The
7 exclusion criteria were (i) patients who do not agree to participate, (ii) patients lost to follow-up at specific
8 time interval, (iii) patients receiving steroids, anticoagulants, prescription non-steroidal anti-inflammatory
9 medication, calcium-channel blockers, or diphosphonate therapy, (iv) patients with a history of
10 thrombophlebitis, vascular insufficiency, or a recent history of alcoholism or nutritional deficiency.¹¹

11 A total of 21 patients (six males and fifteen females) were randomly selected from mandibular
12 prognathism who underwent bilateral IVRO (42 rami) at the authors' institution between August 2007 and
13 March 2014. The operations were performed by 2 surgeons with a minimum of 20 years of surgical
14 experience in oral and maxillofacial surgery. Patients were then randomly allocated to be treated with
15 LIPUS (12 osteotomies, LIPUS group) or without LIPUS (9 osteotomies, control group) after surgery
16 (Table. 1). At the beginning of the study, the first patient to be accepted was assigned to the active treatment
17 group. Other patients were assigned to the placebo group or treatment group in an alternating order. The
18 patients' ages ranged from 16 to 54 years, with a mean age of 24.0 ± 1.9 years. The mean setback was 6.8 ± 0.4
19 mm. There was no potential impact of age, sex and the mandibular set back on the present study. All patients

1 underwent IMF with stainless steel wires (0.3 mm) and brackets placed in the maxillary and mandibular
2 arches for 14 days according to the established clinical pathway.

3 *The LIPUS Treatment*

4 Ultrasound was provided by Sonic Accelerated Fracture Healing System 2000 (SAFHS; provided
5 by Teijin Pharma, Tokyo, Japan). Starting 2 days postoperatively, patients in the LIPUS group received one
6 20-minute LIPUS treatment per day for 3 weeks (intensity: 30 mW/cm², burst width: 200 µs, frequency:
7 1.5 MHz). The transducer was located on the angle of the mandibular ramus at the level of the osteotomy
8 and was firmly fixed with a facial bandage (Fig. 1). Coupling gel was used to ensure effective transfer of
9 the acoustic wave to the tissue. After being properly trained on the correct positioning of the device, the
10 LIPUS treatment was self-administered by patients. The use of the LIPUS machine was checked every day
11 while patients were in hospital for 3 weeks.

12 *CT Measurement Procedure*

13 CT examinations were performed for all patients at one month, six months, and one year
14 postoperatively using Aquilion64[®] (Toshiba Medical Systems, Tokyo, Japan) at the Wakaba Imaging
15 Support Center (tube current: 100 mA; scanning time: 3 s; slice thickness: 2 mm; slice width: 2 mm; field
16 of view: 25 cm). The slice plane was parallel to the occlusal plane and the scanned area extended from the
17 floor of the orbit to the inferior border of the mandible. To reduce the data variation, a single author (S.A.)
18 measured CT images of this study. This person was blinded with regard to the treatment received and
19 assessed all CT images obtained from each patient. The raw data was transferred to a dedicated workstation

(Ziostation2 ver.2.1.5.0; Ziosoft, Tokyo, Japan) with technical consultation. Based on the Ueki visualization method,¹² the frontozygomatic line (FZ line) was defined as the line connecting the most lateral points of the bilateral frontozygomatic sutures in the coronal CT images (Fig. 2A, C). The right and left side line (RL line) was defined as the line connecting the most anterior points of the bilateral auricles in the axial CT images (Fig. 2B). Kim et al.¹³ reported that the color maps created from CT images reconstructed with a section width of 2 mm had better image quality and retained more anatomy details than those reconstructed with a section width of 3 mm. Therefore, three-dimensional volumes were reconstructed with slice imaging by multi-planar reconstruction using a section width of 2 mm as described in Fig 2 A-C. All slices were quantified and bone fragment healing methods were clarified. In the axial CT images, we drew a line tangent to the bilateral foramen-mandibular posterior region to separate the posterior areas (Fig. 2D). In the coronal CT images, we extracted only the part of the mandibular bone that contained the cleavage (Fig. 2E). Based on the Hagino visualization method,¹⁴ we determined reference points of Porion (Po), Crest of Articular Eminence (CAE) in the sagittal CT images. We drew a line perpendicular to the Po-CAE line, starting from the top of the coronoid process in the sagittal images to separate CT values of the mandible bone from wisdom teeth (Fig. 2F). Each analysis volume was divided into two sections of CT slices. In the axial CT images, the upper half of CT slices were defined as the Upper Side of the CT slices and the Lower Side was defined as the lower half of CT slices. Similarly for the other directions of the 3D volume, in the sagittal CT images, half of the CT slices were defined as the Interior Side and the other half were defined as the Lateral Side and in the coronal CT images. The Anterior Side and Posterior Side were defined respectively

1 by half of the CT slices taken.

2 CT can be used to obtain the desired information about the morphological changes and the
3 linear attenuation coefficient of bone density is measured in Hounsfield units (HU). The CT values are
4 correlated to the bone quality.¹⁵ Misch defined bone quality categories from D1 to D5 based off of HU
5 values.¹⁶ Rokn AR et al. reported that the Misch criteria can characterize the histologic properties of the
6 bone.¹⁷ In the present study, the long-term osseous healing of the cleavage space between bone fragment
7 imaging was shown by color maps coded with CT values in HU. The color grades were classified into five
8 categories using the CT values as follows: >1250 HU, red (D1); 850-1250 HU, yellow (D2); 350-849 HU,
9 green (D3); 150-349 HU, blue (D4) and <150 HU, black (D5) (Fig. 3A). D1 bone is primarily dense cortical
10 bone. D2 bone has dense and thick porous cortical bone on the crest and coarse trabecular bone underneath.
11 D3 bone has thinner porous cortical crest and fine trabecular bone within, and D4 has almost no crestal
12 cortical bone and fine trabecular bone composes almost all of the total volume of bone. The warm colors
13 represent the cortical bone areas with high CT values while the cold colors represent the trabecular bone
14 and the soft tissue areas with low CT values. We measured the mean CT values and rated each color grade
15 in the selection range.

16 *Statistical Analysis*

17 The data collection and statistical analyses were performed using IBM SPSS Statistics for
18 Windows version 22.0 (IBM Corp., Armonk, NY, USA). Data was presented as mean \pm standard deviation
19 (SD). The Mann–Whitney U-test was used to assess the differences in the means between the control and

1 LIPUS groups at each time point. A value of $p<0.05$ was considered statistically significant.

2

3 **Results**

4 During the present study, there were no adverse events in either group of patients. We successfully
5 demonstrated the visualization of the cleavage between bone fragments healing. The color grades of the
6 cleavage between bone fragments increased from D5 to D1 over time (Fig. 3B).

7 There were no significant differences between the control and LIPUS groups in age, sex, or
8 mandibular set back. In the sagittal CT images, the mean CT values of the control group were $1,054\pm18$
9 HU preoperatively, 915 ± 20 HU at one month, 916 ± 20 HU at six months, 952 ± 21 HU at one year. The
10 LIPUS group's values were $1,012\pm13$ HU preoperatively, 994 ± 8 HU at one month, $1,011\pm7$ HU at six
11 months, $1,049\pm12$ HU at one year. In the sagittal CT images, the LIPUS group's CT values were
12 significantly higher than those of the control group at one month ($p<0.05$), six months, and one year
13 ($p<0.01$) postoperatively (Fig. 4A). In the axial CT images, the mean CT values of the control group were
14 $1,006\pm17$ HU preoperatively, 856 ± 18 HU at one month, 880 ± 22 HU at six months, 909 ± 25 HU at one year.
15 The LIPUS group's CT values were 985 ± 15 HU preoperatively, 923 ± 8 HU at one month, 955 ± 10 HU at
16 six months, and $1,002\pm12$ HU at one year. In the axial CT images, the LIPUS group had significantly higher
17 CT values than the control group at one month, six months, and one year ($p<0.01$) postoperatively (Fig.
18 4B). In the coronal CT images, the mean CT values of the control group were $1,002\pm20$ HU preoperatively,
19 862 ± 19 HU at one month, 862 ± 22 HU at six months, and 878 ± 21 HU at one year. The LIPUS group had

1 values of $1,003 \pm 16$ HU preoperatively, 924 ± 10 HU at one month, 930 ± 13 HU at six months, and 963 ± 18
2 HU at one year (Fig. 4C). In the axial CT images and coronal CT images, the mean CT value of the LIPUS
3 group was significantly higher than that of the control group at one month, six months and one year ($p < 0.01$)
4 postoperatively. There were no significant differences between all images at the preoperative time point.

5 The posterior side of the coronal color mapping CT images showed a significantly higher amount
6 of D1 grade area in the LIPUS group compared to the control group at six months ($p < 0.05$) and one year
7 ($p < 0.01$) postoperatively (Fig. 5A). As well, the amount of D4 grade area of the control group was
8 significantly higher than that of the LIPUS group at one year ($p < 0.05$) postoperatively. The anterior side of
9 images showed a higher amount of D1 grade area in the LIPUS group compared to the control group at one
10 year ($p < 0.05$) postoperatively (Fig. 5B). In the lower side of the axial color mapped CT images, the amount
11 of D1 and D2 grade area of the LIPUS group was significantly higher than that of the control group at one
12 month ($p < 0.01$ for D1 grade), six months ($p < 0.05$ for D1 and D2 grade areas), and one year ($p < 0.01$ for D1
13 grade, $p < 0.05$ for D2 grade) postoperatively (Fig. 5C). In the upper side of images, the amount of D1 grade
14 area of the LIPUS group was significantly higher than that of the control group at six months ($p < 0.05$)
15 postoperatively (Fig. 5D). In the lateral side of the sagittal color mapping CT images, the amount of D1
16 grade area of the LIPUS group was significantly higher than that of the control group at one month, six
17 months, and one year ($p < 0.01$) postoperatively (Fig. 5E). The amount of D4 grade area of the control group
18 was significantly higher than that of the LIPUS group at one month, six months, and one year ($p < 0.01$)
19 postoperatively. In the interior side, the amount of D1 grade area of the LIPUS group was significantly

1 higher than that of the control group at six months ($p<0.01$) and one year ($p<0.05$) postoperatively (Fig.
2 5F). There were no significant differences at one month.

3

4 **Discussion**

5 We successfully demonstrated osseous healing in the cleavage between bone fragments after IVRO
6 using quantitative 3D analysis of clinical CT data. The results suggested that LIPUS can increase bone
7 density, offering clinical benefits.

8 Quantitative color mapping of CT extends a wide range of applications in the medical and dental
9 fields. Recently, it has been used to for the evaluation of the arterial enhancement fraction of the liver,^{18,19}
10 diagnosis of coronary artery disease,²⁰ prediction of intra-ascending aorta²¹ and the analysis of bone
11 properties in hip osteoarthritis.²² Meyer et al.²³ provided evidence that assessing the degree and location of
12 osseointegration of dental implants are valid using quantitative color mapping of the CT.

13 Buchtala²⁴ was the first to report the possibility to stimulate osteogenesis with ultrasound in 1950.
14 Since then, LIPUS has demonstrated enhanced fracture healing in animal studies and bone repair in humans.
15 It showed a positive effect on accelerating bone healing of fresh fractures with highly significant evidence
16 in experimental and double-blind, randomized, placebo-controlled studies.^{11, 25} Advantages of the use of
17 this technology are its efficacy, safety, and ease of use. In the United States, the Food and Drug
18 Administration approved the use of low-intensity ultrasound for the accelerated healing of fresh fractures
19 in October, 1994 and for the treatment of established nonunions in February, 2000. Erdogan et al.⁷ suggested

1 that LIPUS improved the bone healing of mandibular fractures in rabbits. LIPUS administration was
2 conducted for 20 minutes daily for 20 days in which ultrasound signal consisted of 1.5 MHz pressure wave
3 administered in pulses of 200 μ s with an average temporal and spatial intensity of 30 mW/cm². We utilized
4 this waveform in our previous study^{5,6} and demonstrated that human MHCs play an important role in
5 mandibular fracture healing and that LIPUS accelerates this effect by stimulating various osteogenic
6 cytokines. The gene expression levels of alkaline phosphatase (ALP), osteocalcin (OC), Bone
7 Morphogenetic Protein-2, 4, 7 (BMP-2, 4, 7), runt-related gene 2 (Runx2), osterix (OSX), osteopontin
8 (OPN), parathyroid hormone receptor 1 (PTHr1), and mineralization were increased in the LIPUS (+)
9 group compared to the LIPUS (-)group (control). Histologic studies proved that LIPUS influences
10 osteoblasts, osteoclasts, chondrocytes and mesenchymal stem cells in bone healing. This evidence was used
11 to select the waveform properties in the present study. Patel et al.⁸ revealed a significant improvement in
12 the healing rate of mandibular fractures by radiographic density findings and a significant, rapid reduction
13 in pain perception in the LIPUS group compared with the control group. Uchida et al.²⁶ showed that LIPUS
14 stimulated vascular endothelium growth factor (VEGF) expression in the experiment using the femoral
15 fracture model of mice. Young et al.²⁷ displayed increased angiogenesis in the form of increased blood
16 vessel formation after the application of LIPUS. Rawool et al.²⁸ found that LIPUS increased blood flow
17 around the fracture and surrounding tissue using Power Doppler imaging for the first 2 weeks after surgery.
18 In the present study, patients in the LIPUS group received daily LIPUS treatments for at least 3 weeks
19 postoperatively. The mean CT values of the LIPUS group were significantly higher than that of the control

1 group at one month ($p<0.05$), six months, and one year ($p<0.01$) postoperatively. Considering the results,
2 it could be hypothesized that the increase in blood flow produced an increase in cellular calcium uptake,
3 resulting in increased protein synthesis, thereby accelerating osseous healing.

4 In many other studies, the LIPUS transducer is usually placed transcutaneously during clinical
5 treatments, hence fractures of superficial bone and deeper bone fractures at different depths are exposed to
6 the ultrasound beam at different axial distances. There has been much research observing near field LIPUS
7 on fractures or cells cultures; Reher et al.²⁹ found that near field LIPUS at an axial distance of 5 mm could
8 stimulate bone formation. Fung et al.³⁰ applied LIPUS at three different axial distance fields to femoral
9 fractured rats and observed that LIPUS augmented callus bone volume and mineralization in far field (130
10 mm), and near field (0 mm) and mid-near (60 mm) field enhanced woven bone formation. Similarly, we
11 found that the increase of D1 grade area in the posterior side was faster than the anterior side in the coronal
12 images. Furthermore, the lower side was faster than the upper side in the axial images. In addition, the
13 lateral side was faster than the interior side in the sagittal images. These results may be due to differences
14 in distance from the LIPUS transducer areas further away from the LIPUS application site yielding slower
15 healing. Our study shows that LIPUS can accelerate osseous healing in three-dimensions in both near field
16 and far field areas.

17 In fracture healing, periosteum is the main source of repairing cells, and mainly contributes to
18 callus formation. Ozaki et al.³¹ reported that the periosteum is important for mediating in the fracture healing.
19 Tam et al.³² demonstrated that the positive stimulatory effect of LIPUS on human periosteal cell culture in

functional activation of bone formation and cellular differentiation. Previously, we observed the long-term osseous healing of the cleavage space between bone fragments after IVRO surgery on the interior and lateral sides.¹⁰ In that study, LIPUS was not applied, hence the recovery of the CT values on the lateral side was less than that observed on the interior side at two years postoperatively. At our institution, the periosteum of the lateral side of the mandible was elevated and not removed, while the interior side was not elevated or removed. We reported that the blood supply from the interior side periosteum may affect the speed of osseous healing. The present study observed that in the lateral side, the amount of D1 grade area in the LIPUS group was significantly higher than that of the control group at one month, six months and one year postoperatively ($p<0.01$). Considering these results, it could be hypothesized that LIPUS stimulated the periosteal bone formation of the lateral side of the mandible. Leung et al.³³ found that the stimulatory effect lasted much longer after LIPUS treatment. The reason is that the level of plasma bone-specific ALP activity remained persistently higher at weeks 12, 18 and 27. They reported that the number of bone-forming cells increased in the early phase and that the activity lasted much longer in the treatment group. Similar results were obtained in the present study.

Our study has limitations. First, our sample size was small and further studies may be required to confirm the results of this study. Second, there is a large range in patients' age. Although patients did not have a history of osteopenia or osteoporosis we did not measure bone mineral density preoperatively. It is possible that there may be potential risk. Third, LIPUS can improve bone density, however the period of the postoperative IMF remains uncertain and should be further studied. Finally, we did not use a sham

1 device in the control group. We could have applied such a device to patients for a stronger placebo group.
2 Further consideration will be needed to draw additional implications. We plan to continue to quantitatively
3 evaluate the process of osseous healing. In conclusion, the results observed in this study suggest that LIPUS
4 can improve bone density, offering clinical benefits. We identified no side effects related to LIPUS
5 treatment. In addition, patients felt no discomfort during therapy. The purpose of this study was to observe
6 the long-term osseous healing using quantitative 3D analysis of clinical CT data which successfully
7 demonstrated detailed osseous healing of the mandible bone in three dimensions. We believe that our
8 findings will contribute to the successful surgical treatment of patients using IVRO in the fields of dentistry
9 and oral surgery.

10

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12 commercial, or not-for-profit sectors.

13

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16 grateful for the assistance given by Kaito Uryu. I would also like to express my gratitude to my family for
17 their moral support and warm encouragement.

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16 **Figure Legend**

17 Figure 1. Position of the Low-Intensity Pulsed Ultrasound (LIPUS) transducer

18 The LIPUS transducer was located on the angle of the mandibular ramus at the level of the
19 osteotomy and was firmly fixed with a facial bandage. Coupling gel was used to ensure effective

transfer of the acoustic wave to the tissue.

Figure 2. Method of measuring three-dimensional quantitative color mapping created by using computed tomography (CT) data

A, C: The FZ line was defined as the line between the most lateral points of the bilateral frontozygomatic sutures.

B: The RL line was defined as the line between the most anterior points of the bilateral auricles.

A-C: Based on the reference point, three-dimensional data were reconstructed with 2 mm width slice imaging by multi-planar reconstruction.

D: We drew a line tangent to the bilateral foramen-mandibular posterior region and measured the posterior areas.

E: We extracted only the part of the mandibular bone that contained the cleavage.

F: We determined reference points of Porion (Po), Crest of Articular Eminence (CAE). We drew the vertical line of Po-CAE line which passed through the top of the coronoid process and measured the posterior areas.

Figure 3. Classification of five color grades

A: Based on the Misch criteria, the color grades were classified into five steps using the CT values.

B: The color grades of the cleavage between bone fragments increased from D5 to D1 over time.

Figure 4. Mean CT values \pm standard deviation in the sagittal images (A), the axial images (B) and coronal images (C).

1 Figure 5. Rating of each color grade in the divided two sections of all slices

2 Percent of area covered by each bone grade in the divided two sections of all slices.

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15 **References**

- 16 1. Pan JH, Lee JJ, Lin HY, Chen YJ, Jane Yao CC, Kok SH. Transverse and sagittal angulations of
17 proximal segment after sagittal split and vertical ramus osteotomies and their influence on the
18 stability of distal segment. J Formos Med Assoc. 2013;112(5):244-52.
19 <https://doi.org/10.1016/j.jfma.2012.02.013>

- 1 2. Hara S, Mitsugi M, Tatemoto Y. Variation of plate fixation for mandibular advancement with intraoral
2 vertical ramus osteotomy using endoscopically assisted intraoral rigid or semi-rigid internal fixation:
3 Case series study: Postoperative condylar seating control for mandibular advancement. J
4 Craniomaxillofac Surg. 2015;43(10):2012-6. doi: 10.1016/j.jcms.2015.09.012.
- 5 3. Pomini KT, Andreo JC, Rodrigues Ade C, de O Gonçalves JB, Daré LR, German IJ, Rosa GM Jr,
6 Buchaim RL. Effect of low-intensity pulsed ultrasound on bone regeneration: biochemical and
7 radiologic analyses. J Ultrasound Med. 2014;33(4):713-7. <https://doi.org/10.7863/ultra.33.4.713>
- 8 4. Schandelmaier S, Kaushal A, Lytvyn L, Heels-Ansdell D, Siemieniuk RA, Agoritsas T, Guyatt GH,
9 Vandvik PO, Couban R, Mollon B, Busse JW. Low intensity pulsed ultrasound for bone healing:
10 systematic review of randomized controlled trials. BMJ. 2017;22;356:j656. doi: 10.1136/bmj.j656.
- 11 5. Huang W, Hasegawa T, Imai Y, Takeda D, Akashi M, Komori T. Low-intensity pulsed ultrasound
12 enhances bone morphogenetic protein expression of human mandibular fracture haematoma-derived
13 cells. Int J Oral Maxillofac Surg. 2015;44(7):929-35. <https://doi.org/10.1016/j.ijom.2015.03.001>
- 14 6. Imai Y, Hasegawa T, Takeda D, Akashi M, Lee SY, Niikura T, Shibuya Y, Kurosaka M, Komori T.
15 The osteogenic activity of human mandibular fracture haematoma-derived cells is stimulated by low-
16 intensity pulsed ultrasound in vitro. Int J Oral Maxillofac Surg. 2014;43(3):367-72.
17 <https://doi.org/10.1016/j.ijom.2013.07.746>
- 18 7. Erdogan O, Esen E, Ustün Y, Kürkçü M, Akova T, Gönlüşen G, Uysal H, Cevlik F. Effects of low-
19 intensity pulsed ultrasound on healing of mandibular fractures: an experimental study in rabbits.

J Oral Maxillofac Surg. 2006;64(2):180-8. <https://doi.org/10.1016/j.joms.2005.10.027>

8. Patel K, Kumar S, Kathiriya N, Madan S, Shah A, Venkataraghavan K, Jani M. An Evaluation of the Effect of Therapeutic Ultrasound on Healing of Mandibular Fracture. *Craniomaxillofac Trauma Reconstr.* 2015;8(4):299-306. <http://dx.doi.org/10.1055/s-0034-1544104>.
9. Schortinghuis J, Ruben JL, Raghoobar GM, Stegenga B. Ultrasound to stimulate mandibular bone defect healing: a placebo-controlled single-blind study in rats. *J Oral Maxillofac Surg.* 2004;62(2):194-201. <https://doi.org/10.1016/j.joms.2003.06.006>
10. Arimoto S, Hasegawa T, Kaneko K, Tateishi C, Furudoi S, Shibuya Y, Komori T. Observation of osseous healing after intraoral vertical ramus osteotomy: focus on computed tomography values. *J Oral Maxillofac Surg.* 2013;71(9):1602. e1-1602.e10. <https://doi.org/10.1016/j.joms.2013.02.021>
11. Heckman JD, Ryaby JP, McCabe J, Frey JJ, Kilcoyne RF. Acceleration of tibial fracture-healing by noninvasive, low-intensity pulsed ultrasound. *J Bone Joint Surg.* 1994;76A:26–34.
12. Ueki K, Hashiba Y, Marukawa K, Nakagawa K, Alam S, Okabe K, Yamamoto E. The effects of changing position and angle of the proximal segment after intraoral vertical ramusosteotomy. *Int J Oral Maxillofac Surg.* 2009;38(10):1041-7. <https://doi.org/10.1016/j.ijom.2009.04.021>
13. Kim KW, Lee JM, Klotz E, Park HS, Lee DH, Kim JY, Kim SJ, Kim SH, Lee JY, Han JK, Choi BI. Quantitative CT color mapping of the arterial enhancement fraction of the liver to detect hepatocellular carcinoma. *Radiology.* 2009;250(2):425-434. <https://doi.org/10.1148/radiol.2501072196>

- 1 14. Hagino H, Sawaki Y, Oda T, Ohkubo H, Yamamoto H, Hibi H, Ueda M. Clinical Study of Intraoral
2 Vertical Ramus Osteotomy -Part.1 Radiologic Study of Proximal Segments-. J.Jaw Deform.1996;
3 6(1):32-40.
- 4 15. Wyatt,C.C.L and Pharoah,M.J. Imaging techniques and image interpretation for dental implant
5 treatment. Int.J.Prosthodont. 1998;11:442-452.
- 6 16. Misch CE. Density of bone: effect on treatment plans,surgical approach,healing and progressive bone
7 loading.Int J Oral Implantol. 1990;6(2):23-31.
- 8 17. Rokn AR, Labibzadeh A, Ghohroudi AAR, Shamshiri AR, Solhjoo S. Histomorphometric Analysis of
9 Bone Density in Relation to Tactile Sense of the Surgeon During Dental Implant Placement.
10 Open Dent J. 2018;31;12:46-52. doi: 10.2174/1874210601812010046.
- 11 18. Park M, Chung YE, Kim KA, Chung WS, Lee HS, Han KH, Kim MJ, Kim KW. Added value of
12 arterial enhancement fraction color maps for the characterization of small hepatic low-attenuating
13 lesions in patients with colorectal cancer. PLoS One. 2015;23;10(2):e0114819.
14 <https://doi.org/10.1371/journal.pone.0114819>
- 15 19. Mahnken AH, Klotz E, Schreiber S, Bruners P, Isfort P, Günther RW, Wildberger JE. Volumetric
16 arterial enhancement fraction predicts tumor recurrence after hepatic radiofrequency ablation of liver
17 metastases: initial results. AJR Am J Roentgenol. 2011;196(5):W573-9. doi: 10.2214/AJR.10.4410.
- 18 20. Wang Q, Qin J, Gai LY, Chen YD, Dong W, Guan ZW, Wang ZG, Sun ZJ, Tian JH. A pilot study on
19 diagnosis of coronary artery disease using computed tomography first-pass myocardial perfusion

imaging at rest. J Zhejiang Univ Sci B. 2011;12(6):485-91. doi: 10.1631/jzus.B1000342.

21. Zhang Q, Xu R1, Sun Q, Zhang H, Mao J, Shan T, Pan W, Deuerling-Zheng Y, Kowarschik M, Beilner J. Exploring the Value of Using Color-Coded Quantitative DSA Evaluation on Bilateral Common Carotid Arteries in Predicting the Reliability of Intra-Ascending Aorta Flat Detector CT-CBV Maps. AJNR Am J Neuroradiol. 2015;36(5):960-6. <https://doi.org/10.3174/ajnr.A4238>

22. Turmezei TD, Treece GM, Gee AH, Fotiadou AF, Poole KE. Quantitative 3D analysis of bone in hip osteoarthritis using clinical computed tomography. Eur Radiol. 2016;26(7):2047-54. doi: 10.1007/s00330-015-4048-x.

23. Meyer J, Sheets CG, Earthman JC. Visualization of osseointegration of maxilla and mandible dental implants. Int J Comput Assist Radiol Surg. 2010;5(1):69-76. <http://dx.doi.org/10.1007/s11548-015-1170-9>

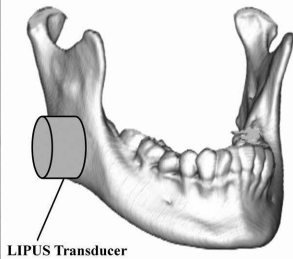
24. Buchtala V. Present state of ultrasound therapy. Dia Med. 1950;22:2944–2950.

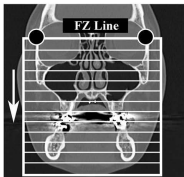
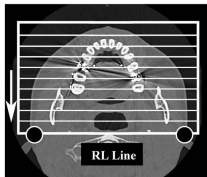
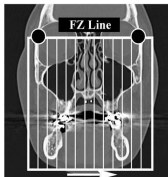
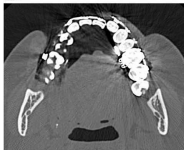
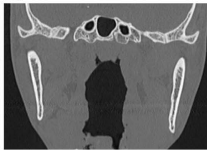
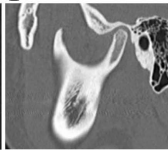
25. Kristiansen TK, Ryaby JP, McCabe J, Frey JJ, Roe LR. Accelerated healing of distal radial fractures with the use of specific, low-intensity ultrasound. A multicenter, prospective, randomized, double-blind, placebo-controlled study. J Bone Joint Surg Am. 1997;79(7):961-73.

26. Uchida K, Urabe K, Naruse K, Mikuni-Takagaki Y, Inoue G, Takaso M. 5. Accelerated Fracture Healing Targeting Periosteal Cells: Possibility of Combined Therapy of Low-Intensity Pulsed Ultrasound (LIPUS), Bone Graft, and Growth Factor (bFGF). J Orthop Trauma. 2016;30(8):S3. doi: 10.1097/01.bot.0000489990.66226.51.

- 1 27. Young SR, Dyson M. The effect of therapeutic ultrasound on angiogenesis. *Ultrasound Med Biol.*
2 1990;16(3):261–269.23.
- 3 28. Rawool NM, Goldberg BB, Forsberg F, Winder AA, Hume E. Power Doppler assessment of vascular
4 changes during fracture treatment with low-intensity ultrasound. *J Ultrasound Med.* 2003;22(2):145-
5 53. <https://doi.org/10.7863/jum.2003.22.2.145>
- 6 29. Reher P, Elbeshir el-NI, Harvey W, Meghji S, Harris M. The stimulation of bone formation in vitro
7 by therapeutic ultrasound. *Ultrasound Med Biol.* 1997;23(8):1251-8.
8 [https://doi.org/10.1016/S0301-5629\(97\)00031-8](https://doi.org/10.1016/S0301-5629(97)00031-8)
- 9 30. Fung CH, Cheung WH, Pounder NM, de Ana FJ, Harrison A, Leung KS. Investigation of rat bone
10 fracture healing using pulsed 1.5 MHz, 30 mW/cm(2) burst ultrasound--axial distance dependency.
11 *Ultrasonics.* 2014;54(3):850-9. <https://doi.org/10.1016/j.ultras.2013.10.013>
- 12 31. Ozaki A, Tsunoda M, Kinoshita S, Saura R. Role of fracture hematoma and periosteum during fracture
13 healing in rats: interaction of fracture hematoma and the periosteum in the initial step of the healing
14 process. *J Orthop Sci.* 2000;5(1):64-70. <https://doi.org/10.1007/s007760050010>
- 15 32. Tam KF, Cheung WH, Lee KM, Qin L, Leung KS. Osteogenic effects of low-intensity pulsed
16 ultrasound, extracorporeal shockwaves and their combination - an in vitro comparative study on
17 human periosteal cells. *Ultrasound Med Biol.* 2008;34(12):1957-65.
18 <https://doi.org/10.1016/j.ultrasmedbio.2008.06.005>
- 19 33. Leung KS, Lee WS, Tsui HF, Liu PP, Cheung WH. Complex tibial fracture outcomes following

1 treatment with low-intensity pulsed ultrasound. *Ultrasound Med Biol.* 2004;30(3):389-95.
2 <https://doi.org/10.1016/j.ultrasmedbio.2003.11.008>
3
4

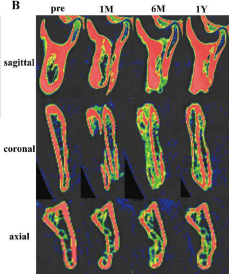


A**B****C****D****E****F**

A Misch criteria

grade	color	CT values(HU)
D1	red	>1250
D2	yellow	850-1250
D3	green	350-849
D4	blue	150-349
D5	black	$150 >$

B





Group	Control	1M-LPS	4M-LPS	1Y-LPS
LPS	Control	LPS	LPS	Control



Group	Control	1M-LPS	4M-LPS	1Y-LPS
LPS	Control	LPS	LPS	Control



Group	Control	1M-LPS	4M-LPS	1Y-LPS
LPS	Control	LPS	LPS	Control

* P < 0.05 ** P < 0.01

